Detection of Gliadin in Foods Using a Quartz Crystal Microbalance Biosensor That Incorporates Gold Nanoparticles

Pei-Tzu Chu,‡ Chih-Sheng Lin,§ Wei-Jung Chen,® Chih-Feng Chen,‡ and Hsiao-Wei Wen*†

‡Department of Food Science and Biotechnology, National Chung Hsing University, Taichung, Taiwan, Republic of China
§Department of Biological Science and Technology, National Chiao Tung University, Hsinchu, Taiwan, Republic of China
®Institute of Biotechnology, National I-Lan University, I-Lan, Taiwan, Republic of China
‡Department of Animal Science, National Chung Hsing University, Taichung, Taiwan, Republic of China

ABSTRACT: This work develops a label-free gliadin immunosensor that is based on changes in the frequency of a quartz crystal microbalance (QCM) chip. A higher sensitivity was obtained by applying 25 nm gold nanoparticles (AuNPs) to the surface of a bare QCM electrode. Subsequently, chicken anti-gliadin antibodies (IgY) were immobilized directly on the AuNP-modified surface by cross-linking amine groups in IgY with glutaraldehyde. Experimental results revealed that the change in frequency exhibited when 2 ppm gliadin was bound to the AuNP-modified electrode was 35 Hz (48%) greater than that of the bare gold electrode. The linear dynamic range in 60% ethanol was from $1 \times 10^1$ to $2 \times 10^3$ ppb gliadin, and the calculated limit of detection (LOD) was 8 ppb. The entire detection process was completed in 40 min and was highly repeatable. Additionally, the AuNP-modified QCM system generated results in the detection of gliadin in 10 commercial food products that were consistent with those obtained using an AOAC-approved gliadin kit. In conclusion, the QCM platform provides a potential alternative means of ensuring that people with wheat allergies and celiac patients have access to gliadin-free food.

KEYWORDS: gliadin, quartz crystal microbalance immunosensor, gold nanoparticles

INTRODUCTION

Cereals and cereal products are important food resources for human beings. As well as serving as a major energy source, owing to their high carbohydrate content, cereals are also vital sources of vitamins, minerals, soluble and insoluble dietary fibers, and proteins. Of all of the cereals, wheat is not only a particularly important cultivated crop but also an allergenic food. In the United States, wheat-related food allergies constitute approximately 2.5% of all food allergies in children. In France, wheat ranks as the 8th most common food allergen in children and the 12th most common in adults; 14–20% of the entire French population with a food allergy is allergic to wheat. Although rice is a staple food in Asia, wheat products such as noodles and bread are still widely consumed. Consequently, wheat is also responsible for a significant proportion of food allergies in Asia. Following eggs and dairy milk, wheat ranks as the third food allergen in Japan. In eastern Taiwan, wheat allergies constitute around 5.4% of all food allergies in children.

Wheat gluten is composed of many alcohol-soluble proteins, of which the main one is gliadin. Gliadin is a major allergen that is responsible for gluten intolerance, bakers’ asthma, and wheat-dependent exercise-induced anaphylaxis. Celiac disease (CD) is a genetically determined autoimmune disease of the digestive system, which results in chronic inflammation of the gastrointestinal tract. CD flattens the small intestinal mucosa, hindering nutrient absorption. The condition can be reversed by a gluten-free diet. Previous studies have demonstrated that the safe limit on ingested wheat protein is higher for wheat-allergic patients than for celiac patients. Because the sensitivity to gluten varies among individuals, it is not easy to set an acceptable limit on trace amounts of gluten in gluten-free foods. Recently, the official limit set by regulation (EC) No. 41/2009 of the European Union for all foodstuffs except infant formulas is currently <20 mg/kg of gluten in gluten-free foods and 20–100 mg/kg of gluten in very low-gluten content food. Therefore, highly sensitive assays are crucial for detecting gluten contaminants in gluten-free food.

Numerous methods for detecting wheat allergens have been established. They are mass spectrometry, the polymerase chain reaction (PCR), real-time PCR, and immunological tests. For example, a biosensor that is based on a fluorescence assay was used to detect the amino acid sequence XXQPQPQQQQQQQQQQQQL, which is represented in gliadin and other prolamins and is considered to be toxic to celiac patients. This sensor exhibited a linear response between 2.0 and 8.0 μM gliadin. An electronic tongue has previously been developed for the semiquantitative detection of gliadin with a sensitivity of 1–2 mg/kg of gliadin in baby milked flour. A standard quantitative method is required to determine the gluten concentration in food. Two officially approved enzyme-linked immunosorbent assay (ELISA) kits have been developed to quantify native and heated gluten. The first commercial kit, approved by the Association of Official Analytical Chemistry (AOAC), uses a monoclonal antibody to detect α-gliadin, whereas the second one, approved by the Codex Alimentarius Commission, utilizes an R5 monoclonal antibody to detect α-gliadin, β-gliadin, and γ-gliadin. These kits are commonly used to evaluate the gluten content of various food products.
antibody to react with the celiac toxic epitope of gliadin, QQPFP.21 However, these gliadin analysis systems are time-intensive, inconvenient, and expensive and require that their operators have been extensively trained. Therefore, a rapid, sensitive, user-friendly, and environmentally friendly analytical system must be developed for detecting gliadin in foods.

Some label-free methods, including surface plasmon resonance (SPR) and quartz crystal microbalance (QCM), have been developed.22 In 1959, Sauerbrey established the relationship between the change in resonant frequency of quartz and the change in mass of attached molecules on the surface of a gold electrode in a QCM, leading to the development of QCM as a commonly used biosensor that depends on the increase in mass that is caused by the absorption of target molecules.23,24 As a directly responsive microsensor, QCM is extensively applied in the liquid phase system uses AuNPs as carriers and is adopted in the better detection limit. For example, the QCM DNA sensing electrode in the QCM with AuNPs. The changes in frequency caused by the mass on a QCM chip by modifying the surface of the gold electrode in the QCM with AuNPs. The changes in frequency (ΔF) and assay sensitivity of this developed QCM were compared with those of the traditional QCM with an unmodified gold electrode.

MATERIALS AND METHODS

Materials. Wheat, barley, oat, rice, foxtail millet, corn, buckwheat, and soybean were purchased from local supermarkets (TaiChung, Taiwan). Wheat gliadin, hydrogen tetrachloroaurate (III) trihydrate, sodium citrate, glutaraldehyde, cysteamine, glycine, polyethylene glycol 10000 (PEG10), and other chemicals were purchased from Sigma-Aldrich Co. (St. Louis, MO, USA). A QCM sensor, 9 MHz AT-cut quartz and the change in mass of attached molecules on the surface of a gold electrode in a QCM, leading to the development of QCM as a commonly used biosensor that depends on the increase in mass that is caused by the absorption of target molecules.23,24 As a directly responsive microsensor, QCM is extensively applied in the liquid phase system uses AuNPs as carriers and is adopted in the better detection limit. For example, the QCM DNA sensing electrode in the QCM with AuNPs. The changes in frequency caused by the mass on a QCM chip by modifying the surface of the gold electrode in the QCM with AuNPs. The changes in frequency (ΔF) and assay sensitivity of this developed QCM were compared with those of the traditional QCM with an unmodified gold electrode.

Preparation of Wheat Protein Sample. Wheat protein was extracted using two methods. The first was ethanol extraction, and the other involved the RIDA extraction buffer by following the manufacturer’s instructions. In the ethanol extraction method, wheat flour (1 g) was rotatively mixed with 10 mL of reverse osmosis water (RO) for 1 h at room temperature. After centrifugation at 5000 rpm for 10 min, the pellet was formed and was extracted with 10 mL of 60% ethanol for 1 h to obtain gliadin. In the second method, the RIDA extraction solution (2.5 mL) in the RIDASCREEN Gliadin kit (R-Biopharm AG) was added to 0.25 g of wheat flour and mixed for 40 min at 50 °C, and this mixture was then reacted with 7.5 mL of 80% (v/v) ethanol for 1 h at room temperature. The mixture was centrifuged at 5000 rpm for 10 min at room temperature to collect the supernatant that contained the extracted gliadin. Additionally, a commercially bought gliadin (Sigma-Aldrich Co.) was used to prepare a standard gliadin solution.

Immunization of Hens. The white Leghorn hen lays eggs continually throughout the year, approximately 280 egg/year, and so was adopted herein to obtain egg yolk immunoglobulin (IgY). Hens were immunized following the procedure of Kim et al.35 Eight 40-week-old white Leghorn hens were kept in standard facilities for poultry farming and provided with food and water. To investigate the preimmune background, eggs were collected before the first injection. The Leghorn chicken was vaccinated in the thorax muscle at two sites using 1.5 mL of gliadin-complete Freund’s adjuvant mixture. The antigen mixture that was used in the first injection was prepared by mixing 0.5 mL of the gliadin standard solution (1 mg/mL) with 1 mL of the complete Freund’s adjuvant. After 14 days, a second boost injection was given. In the second injection, incomplete Freund’s adjuvant replaced complete Freund’s adjuvant. Eggs were collected daily throughout the immunization period until 1 week after the third boost, and each was stored at 4 °C until use.

Preparation of Anti-gliadin IgY from Yolk. Anti-gliadin IgY was isolated from gliadin-immunized chicken eggs using three methods, which were the chloroform—PEG method,36 the PEG—alcohol (PEG-Alc) method,37 and the water dilution method.38 The PEG—Alc method is explained briefly herein because this study mainly used this method to isolate IgY from eggs. First, the egg yolk was washed gently with clean water to remove as much egg white as much as possible. A volume of 3.5% PEG10 in 0.1 M phosphate buffer saline (PBS, pH 7.6) that was 4 times the volume of the egg yolk was mixed with the yolk. Following stirring, the mixture was centrifuged at 8000 rpm for 10 min, and more PEG10 was added to the clear supernatant to obtain a final concentration of 12% (w/v). After the mixture had been centrifuged at 8000 rpm for an additional 10 min, the supernatant was removed and the pellet was dissolved in a PBS equivalent to half of the volume of the original yolk/PBS mixture. PEG10 was then added to a final concentration of 12% (w/v). The mixture was centrifuged again at 8000 rpm for 10 min, and the supernatant was removed. The pellet was then dissolved in PBS and 50% ethanol with a total volume of half of the original volume of the yolk. Next, the extract was centrifuged, and the pellet was dissolved in 1 mL of PBS before being dialyzed against PBS for 24 h. Finally, the concentration, titer, and purity of IgY were estimated with protein assay (at 280 nm), ELISA, and Western blot analysis, respectively.

Preparation of AuNPs. The solution of AuNPs was obtained by the reduction of HAuCl₄ using citrate, as described by Sarasua et al.39 Fifteen milliliters of deionized water was added to 10 mL of 0.1% HAuCl₄ in an oil bath. After the temperature had reached 120 °C, a volume (3.06, 2.42, or 0.88 mL) of 38.8 M sodium citrate was rapidly added to yield differently sized AuNPs. A color change from dark blue to wine-red revealed the formation of AuNPs. Next, the size of the AuNPs was measured by laser diffraction particle size analysis in a light-scattering particle size analyzer (Coulter Scientific Instruments, Hialeah, FL, USA). Finally, the AuNPs were stored at 4 °C until use.

Optimization of QCM Biosensor. The QCM biosensor was optimized by applying various concentrations (100, 200, or 300 μg/mL) of polyclonal anti-gliadin IgY onto the AuNP-modified chip at various flow rates (5, 10, 20, or 60 μL/min) through the QCM chips. The flow rate was controlled by the flow injection system, and the entire QCM system was purchased from ANT Technology Co., Ltd. (Taipei, Taiwan). Two methods for immobilizing IgY on the surface of the gold electrode are (i) the direct immobilization of IgY onto the electrode and (ii) the indirect immobilization of IgY onto the electrode via the immobilization of AuNPs. Herein, method (i) involved directly fixing the anti-gliadin IgY onto the gold electrode surface with glutaraldehyde and then blocking with 1 M glycine. In method (ii), the electrode was first coated with AuNPs by using glutaraldehyde and cysteamine as linkers. Following the immobilization of AuNPs on the electrode, 0.5 M cysteamine was again injected to form the NH₂ groups on the AuNP surface. The anti-gliadin IgY was then attached to the surface of AuNPs using 2.5 M glutaraldehyde. Between each step of the immobilization process, the electrode surface was washed until a
constant frequency was obtained. Scheme 1 illustrates each step of the surface modification of the QCM gold electrode using method ii. Distilled water (18.2 MΩ cm) was used as the running buffer, and the change in frequency was determined using the developed QCM system.

Assay Procedure. The specificity of this developed QCM assay was using alcohol-soluble proteins (prolamins) that were extracted from various cereal samples (wheat, barley, oat, rice, foxtail millet, corn, buckwheat, and soybean). All cereals were milled to produce flour, and impurities were removed by sifting through a 100 mesh screen. The albumins and the globulins in 5 g of cereal flour were removed using deionized water and 0.5 M NaCl solution, respectively. Following the extraction of the pellet with 60% (v/v) ethanol, the supernatant was filtered through a 0.45 μm pore sized filter. The standard gliadin from wheat was diluted with 60% ethanol serially at concentrations from 1 × 10^5 to 2 × 10^5 ppb (ng/mL) to obtain an optimized standard curve. The repeatability of the QCM assay was ensured by performing the experiment using different chips at three concentrations of gliadin (10, 100, and 1000 ppm). Moreover, to confirm the feasibility of this developed QCM assay in detecting gliadin in real food samples, it was applied to analyze 10 commercial food products, including 4 gluten-free foods (pancake mix, custard mix, baby rice, and buckwheat). The results were compared with those presented in Figure 1a.

Statistical Analysis. All data obtained using the developed QCM assay are presented as the mean ± standard deviation (SD). Statistical analyses were performed with the use of the SAS statistical package (SAS Institute, Cary, NC, USA). A p value under 0.05 was considered to indicate significance.

RESULTS AND DISCUSSION

Preparation and Characterization of Anti-gliadin IgY. To extract a large amount of chicken IgY antibody from egg yolk, three purification methods were adopted in this study. They were the chloroform−PEG method, the PEG−Alc method, and the water dilution method. Figure 1a presents the variety of purified egg proteins that were analyzed using the 12% SDS-PAGE. In lanes A, C, and E were the egg proteins from the control egg that were collected before immunization, and in lanes B, D, and F were the egg proteins after the first boost. The results from lanes B, D, and F reveal a higher concentration of IgY than in the corresponding control eggs (lanes A, C, and E). The chloroform−PEG method (lanes A and B) and the water dilution method (lanes E and F) very effectively extracted the antibody IgY from the yolk, and the PEG−Alc method (lanes C and D) yielded clear bands for the heavy chain and the light chain of IgY antibodies with the correct molecular weights. Hence, the PEG−Alc method was chosen as the optimal method for isolating IgY from egg yolk. The purified antibodies from the egg yolks of the eggs collected before immunization (n = 3) were 34 ± 2 IgY mg/mL. The first boost increased the antibody concentration to 90 ± 13 mg/mL, and the second boost increased it to 188 ± 10 mg/mL. Additionally, Figure 1b displays the profiles of wheat proteins that were extracted through various methods and the Western blot images with the use of isolated anti-gliadin IgY through the PEG−Alc method. In lane 1 were water-soluble wheat proteins; in lanes 2 and 3 were ethanol-soluble wheat proteins obtained by different extraction methods (lane 2, 60% ethanol; lane 3, RIDA extraction solution), and in lane 4 was the gliadin standard from Sigma-Aldrich Co. Wheat gliadin molecules can be divided into a high molecular weight (HMW) group (67–70 kDa), a medium molecular weight (MMW) group (55–59 kDa), and a low molecular weight (LMW) group, which includes α/β- and γ-gliadins (28–39 kDa). Sixty percent ethanol (lane 2) could extract a higher amount of α-gliadin than RIDA extraction solution (lane 3). The isolated anti-gliadin IgY recognized only α-gliadin in lanes 2–4 and did not react with any of the water-soluble wheat proteins in lane 1. Accordingly, the isolated anti-gliadin IgY antibody in this work could specifically distinguish α-gliadin from other proteins in wheat.
Immobilization of IgY on QCM Surface with AuNPs. Nanostructure possesses a high surface-to-volume ratio, and this unique property can provide a nanoparticle-modified electrode a chance to coat a larger amount of antibodies and then give the coated antibodies three-dimensional directions to increase the likelihood of antibody–antigen interaction. These favorable properties increase the sensitivity of an immunoassay. Therefore, to increase the sensitivity of the QCM in the detection of gliadin, a novel immobilization method for increasing the number of IgY binding sites on a QCM chip using AuNPs, shown as Scheme 1, is developed herein. As the molar ratio of sodium citrate/HAuCl₄ decreased, larger AuNPs were obtained. When a mixture of 15 mL of deionized water and 10 mL of 0.1% HAuCl₄ was added to different volumes of 38.8 mM sodium citrate (3.06, 2.42, or 0.88 mL), AuNPs were formed with sizes of 17, 25, or 40 nm, respectively (data not shown). Figure 2A summarizes the results of the assay processing. Each arrow indicates the attachment of a different material to the surface of the QCM. Initially, in stage a, 2.5 M glutaraldehyde was added and the carbonyl groups of glutaraldehyde interacted with the amino groups on the chip by a cross-linking reaction. Then, in stage b, the carbonyl group on the chip reacted with the cysteamine. In stage c, the AuNPs were added and interacted with the sulphydryl group of the bound cysteamine. The consequent increase in mass yielded a ΔF around 300 Hz, and a signal with a steady frequency was thus achieved. Following a series of chemical modifications on the AuNPs (stages d and e), the anti-gliadin antibody was attached to the AuNPs in stage f. A steady interaction thus occurred between the amino groups of the antibodies and the carboxyl groups on the AuNP-modified chip, and the frequency was reduced again to approximately 680 Hz. Finally, the vacant, active sites on the chip were blocked using 1 M glycine.

Figure 2B displays the effect of AuNP size on the binding quantity of antibodies and the assay signal as detecting 2 ppm gliadin. Generally, ΔF increased with the size of AuNPs that coated the chip. Relative to the bare and AuNP-modified chips, coating antibody on the 17, 25, and 40 nm AuNP chips changed the frequency by 120 ± 2, 170 ± 6, and 109 ± 3 Hz, respectively. The decrease in the frequency of the 40 nm AuNP modified chip may have been caused by the aggregation of 40 nm AuNPs on the chip when the flow rate of the injection system was 10 μL/min. Therefore, the coating of 25 nm AuNPs onto the chip was optimal, and the signal (ΔF) was 106 ± 5 Hz in the detection of 2 ppm gliadin. Compared with the bare gold electrode, the increase in frequency when 2 ppm gliadin was detected using the 25 nm AuNP-modified electrode was 35 Hz (48%). The SEM results demonstrate that all of the AuNPs that coated the surface of the QCM chip had similar sizes around 25 nm, with the aggregation of a few AuNPs (Figure 3).

Table 1 presents the change in frequency, the corresponding change in mass, and surface coverage by various molecules upon the modification of the bare gold electrode or the AuNP-modified electrode of the QCM. The corresponding change in mass was calculated using the Sauerbrey equation,

\[
\Delta F = \frac{-2\Delta m f^2}{A \sqrt{\mu \rho}} = -C \Delta m
\]

where \(C\) is a constant, f is intrinsic crystal frequency (9 MHz), A is piezo-electrically active area (0.091 cm²), \(\rho = 2.65 \text{ g/cm}^3\), and \(\mu\) is shear modulus of
the developed QCM biosensor. 

10 detecting target molecules also provided assays that are based on the use of nanotubes as a medium for impossibility to calculate its surface coverage. 

\[
\text{Hz and the surface coverage of IgY from 3.1} \times 10^9 \text{ to 179 g/cm}^2 \text{ (} 1.7 \text{ times). These results reveal that the gold nanoparticles increased the IgY binding capacity. This finding was consistent with a study in which the deposition of AuNPs on an electrode in an electrochemical biosensor substantially increased the sensitivity of the biosensor to arsenite.43 Other assays that are based on the use of nanotubes as a medium for detecting target molecules also provided amplified assay signals.44–46 Hence, this work also demonstrated that adding AuNPs to a QCM chip provided additional spaces for the immobilization of antibodies, increasing the change in frequency of the assay. }

Optimization of Assay Time by Controlling Flow Rate of the QCM System. The flow rate and the duration of interaction of molecules with the sensor system critically affect the sensitivity of a flow injection mode sensor system.47,48 Accordingly, an attempt was made herein to reduce the time required to analyze 2 ppm gliadin while retaining the sensitivity of the assay by optimizing the flow rate through the AuNP-modified chip (Figure 4A). According to Figure 4B, when the flow rate was maintained at 60 μL/min, although the assay could be completed in 10 min, the frequency only slightly changed. Setting the flow rate at a lower value increased the change in frequency, perhaps by increasing the contact time in which IgY could interact with the gliadin. However, completing an assay at a lower flow rate took longer. According to the inset figure, the optimal detection flow rate in this assay was 10 μL/min, which yielded the largest change in frequency, 108 Hz, with an assay time of about 40 min. 

Repeatability of the Detection of Gliadin by QCM Biosensor. A detection platform must be stable and ensure that any experiment in which it is used can be repeated or reproduced accurately. Hence, the repeatability of the developed QCM assay must be evaluated. The repeatability is reproduced accurately. Hence, the repeatability of the 

Table 1. Changes of Parameters in Each Step of Modification of QCM Chip

<table>
<thead>
<tr>
<th>modification step</th>
<th>MW (g/mol)</th>
<th>frequency change ((\Delta f); Hz)</th>
<th>mass change ((\Delta m); ng)</th>
<th>surface coverage ((\Gamma); mol/cm²)</th>
</tr>
</thead>
<tbody>
<tr>
<td>bare electrode</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>(a) 2.5 M glutaradehyde</td>
<td>100.12</td>
<td>148.1 ± 2.3</td>
<td>72.7 ± 0.8</td>
<td>8.1 \times 10^{-9}</td>
</tr>
<tr>
<td>(b) anti-gliadin IgY</td>
<td>180000</td>
<td>103.5 ± 4.9</td>
<td>51.4 ± 1.5</td>
<td>3.1 \times 10^{-12}</td>
</tr>
<tr>
<td>(c) 1 M glycine</td>
<td>75.07</td>
<td>20.1 ± 3.5</td>
<td>10.1 ± 1.2</td>
<td>1.5 \times 10^{-9}</td>
</tr>
<tr>
<td>(d) 20 ppm gliadin</td>
<td>55–39</td>
<td>72.1 ± 0.2</td>
<td>23.5 ± 0.1</td>
<td>–a</td>
</tr>
<tr>
<td>AuNP-modified electrode</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>(a) 2.5 M glutaradehyde</td>
<td>100.12</td>
<td>149.3 ± 5.6</td>
<td>69.2 ± 3.1</td>
<td>8.1 \times 10^{-9}</td>
</tr>
<tr>
<td>(b) 0.5 M cysteamine</td>
<td>77.15</td>
<td>88.7 ± 4.7</td>
<td>44.1 ± 1.7</td>
<td>5.7 \times 10^{-9}</td>
</tr>
<tr>
<td>(c) AuNP</td>
<td>–b</td>
<td>75.4 ± 7.7</td>
<td>37.5 ± 2.7</td>
<td>–b</td>
</tr>
<tr>
<td>(d) 0.5 M cysteamine</td>
<td>77.15</td>
<td>65.5 ± 6.3</td>
<td>32.5 ± 2.2</td>
<td>4.6 \times 10^{-9}</td>
</tr>
<tr>
<td>(e) 2.5 M glutaradehyde</td>
<td>100.12</td>
<td>81.4 ± 4.8</td>
<td>40.5 ± 1.7</td>
<td>4.4 \times 10^{-9}</td>
</tr>
<tr>
<td>(f) anti-gliadin IgY</td>
<td>180000</td>
<td>178.7 ± 9.4</td>
<td>88.6 ± 3.3</td>
<td>5.4 \times 10^{-12}</td>
</tr>
<tr>
<td>(g) 1 M glycine</td>
<td>75.07</td>
<td>45.2 ± 6.4</td>
<td>22.5 ± 2.2</td>
<td>3.3 \times 10^{-9}</td>
</tr>
<tr>
<td>(h) 20 ppm gliadin</td>
<td>55–39</td>
<td>106.8 ± 5.4</td>
<td>36.1 ± 2.7</td>
<td>–a</td>
</tr>
</tbody>
</table>

“Not available; gliadin was the complex as the ethanol-soluble wheat proteins with the molecular weight range as 39–55 kDa, resulting in the impossibility to calculate its surface coverage.44 Not available; the gold nanoparticle (AuNP) was the polymer for which a molecular weight was not available, resulting in the impossibility to calculate the surface coverage of AuNP.

Figure 4. Effect of flow rate (5, 10, 20, and 60 μL/min) on changes in frequency (A) and detection time (B) in detection of 2 ppm of gliadin using the developed QCM biosensor.
AuNP-modified QCM chip revealed no variation in the baseline among the runs, indicating that the IgY molecules that were coated on the AuNP-modified chip were very stably immobilized. Furthermore, 10, 100, and 1000 ppb gliadin were continually analyzed in an AuNP-modified chip, and this procedure was repeated in triplicate using three individual chips. Figure 5B displays the results thus obtained. The mean ΔF was determined to be 26 ± 3, 65 ± 3, and 95 ± 5 Hz for 10, 100, and 1000 ppb gliadin, respectively. The reliability was calculated using the relative standard deviation (%RSD), which was 12.2, 4.9, and 5.6% with 10, 100, and 1000 ppb gliadin, respectively. All of the RSD values in this test were <15%, indicating the feasibility of this developed immunosensor. These findings demonstrate that the proposed QCM with the AuNP-modified chip provides consistent and satisfactory analytical results with respect to gliadin.

**Assay Sensitivity.** The sensitivity of the proposed method was evaluated on the basis of the detection of gliadin at various concentrations (1 × 10<sup>1</sup>−2 × 10<sup>5</sup> ppb) in 60% ethanol. The limit of detection (LOD) and the limit of quantitation (LOQ) of this assay were determined from the dose–response curve (Figure 6). The LOD and LOQ were defined as the least concentration of analytes that could be distinguished from the background signal by 3 and 10 standard deviations of the baseline noise, respectively. The R² values of the dose–response curves of bare and AuNP-modified QCM chips were 0.953 and 0.997; the LOQ values were 26 and 11 ppb, and the LOD values were estimated to be 22 and 8 ppb, separately. The slope of the standard curve represented the sensitivity of the assay, and the AuNP-modified chip was associated with a greater value (39.584 vs 30.113). Therefore, the AuNP-modified chip was utilized in the final assay in this study.

Numerous methods for detecting gliadin have been reported. Three ELISAs using anti-gliadin monoclonal antibodies had different LOD values, 3.2 ppm for R5-ELISA, ≥150 ppm for AOAC-ELISA, and 1.5 ppm for a sandwich ELISA using two monoclonal antibodies. The LOD of a nonimmune assay in the detection of gliadin using a microfluorimeter was 4.1 ppm; that of a fluorescence correlation spectroscopy assay was 60 ppb gliadin. The use of the AuNP-modified chip gave this QCM biosensor a low LOD of 8 ppb in detecting gliadin and, so, improved protection against accidental contamination of gliadin-free food products by gluten.

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**Figure 5.** (A) Repeatability of nonstop analysis of negative control (60% ethanol) using a AuNP-modified chip. Three concentrations of gliadin (10, 100, and 1000 ppb) were continually analyzed in an AuNP-modified chip, and this procedure was repeated in triplicate using three individual chips. (B) The change in frequency and RSD associated with each gliadin concentration were calculated.

**Figure 6.** Two dose-response curves of gliadin in 60% ethanol. Solid and dotted lines are regression lines obtained using the developed QCM with the AuNP-modified chip or the bare chip, respectively. LOD of the bare chip was calculated to be 22 ppb gliadin, and R² was 0.953. LOD of the AuNP-modified chip was calculated to be 8 ppb gliadin, and R² was 0.997.
Practical Applications of QCM Biosensor in Real Food Samples. Because the anti-gliadin antibodies from the yolk that was used in the assay developed herein were polyclonal, the specificity of this assay must be evaluated. Most related works have tried to identify gliadin-free food by quantifying the gliadin in a test sample.\textsuperscript{15,53} Therefore, in this work, eight cereal samples were processed to remove the water-soluble albumins and salt-soluble globulins before extraction with 60% ethanol to obtain gliadin in samples.\textsuperscript{56–58} Figure 7 summarizes the results of the QCM assays of cereals that underwent extraction using 60% ethanol. Besides wheat, only barley showed a significant frequency change among the other seven cereals (Figure 7A). With the percentage change in frequency ($\Delta F\%$) in the detection of gliadin in wheat defined as 100%, that in the detection of barley was 35% (Figure 7B). This cross-reactivity might have been caused by the binding of polyclonal anti-gliadin IgY antibodies to structurally similar epitopes in barley, which are homologous with those in wheat or contain sequences identical or nearly identical to those in wheat. Hence, the cross-reactivity between wheat and barley can be explained with reference to taxonomic relationships among various species of the same family that have strong protein sequence similarities.\textsuperscript{59,60} On average, the results concerning the specificity of this developed assay are satisfactory for the other considered cereals, which are oat, foxtail, millet, rice, corn, buckwheat, and soybean.

The recovery rate reflected the efficiency of extraction of gliadin upon measurement following the addition of a known amount of gliadin to a real food sample. Gliadin-free spaghetti in tomato sauce was spiked with gliadin (1–1000 ppm) to determine its rate of recovery. Figure 8 summarizes the results concerning the recovery rate. When 1 ppm gliadin was added, a
low recovery rate (25%) was obtained. However, when 10–
1000 ppm gliadin was added, the recovery rates were close to
100% (98–107%). The direct approach to detect gliadin in
food is effective from 1 to 1000 ppm of gliadin (R² = 0.996)
with the detection limit as 1 ppm of gliadin. The results indicate
that the combination of this extraction method with the
developed QCM assay using the AuNPs-modified chip can be
used for detecting gliadin in food samples, because its detection
limit is lower than the official limit of gluten-free foods that has
been set by the European Commission of 20 ppm of gluten,
which equals 10 ppm of gliadin. In addition, the minimum
detectable concentration of gliadin in the food matrix using this
developed QCM assay exceeded that in the buffer environment,
perhaps because of disturbance of the sample matrix by fat,
carbohydrate, and other entities, probably blocking the
antibody binding sites and then affecting the antibody–antigen
interaction. These factors may have affected the performance
of the assay, reducing its sensitivity. Table 2 presents the

Table 2. Specificity and Sensitivity of QCM in Detection
of Gliadin at Three Levels of Contamination in a Foodstuff
(Buckwheat)

<table>
<thead>
<tr>
<th>actual group</th>
<th>predicted group</th>
<th>gliadin-free</th>
<th>low-gliadin content</th>
<th>gliadin-containing</th>
<th>total</th>
<th>sensitivity (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>gliadin-free</td>
<td>7</td>
<td>2</td>
<td>0</td>
<td>9</td>
<td>78</td>
<td></td>
</tr>
<tr>
<td>low-gliadin content</td>
<td>0</td>
<td>6</td>
<td>3</td>
<td>9</td>
<td>67</td>
<td></td>
</tr>
<tr>
<td>gliadin-containing</td>
<td>0</td>
<td>0</td>
<td>9</td>
<td>9</td>
<td>100</td>
<td></td>
</tr>
<tr>
<td>total</td>
<td>7</td>
<td>8</td>
<td>12</td>
<td>27</td>
<td></td>
<td></td>
</tr>
<tr>
<td>specificity (%)</td>
<td>100</td>
<td>75</td>
<td>75</td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

sensitivity and specificity of the three gliadin contamination
levels in a single foodstuff (buckwheat). “Gliadin-free”, “low-
gliadin”, and “gliadin-containing” refer to gliadin concentrations
in the foodstuff of <10, 10–100, and >100 ppm, respectively.
The false-negative rate in the low-gliadin and gliadin-containing
food samples and the false-positive rate in the gliadin-free
sample were 0 and 22%, respectively.

Products for gluten-free diets are becoming more available
globally. In food factories with poor quality control, cross-
contamination with wheat may be serious. Therefore, detecting
wheat contamination is the top priority for manufacturers of
gluten-free food products. To test the feasibility of the
developed QCM assay in the detection of real food samples,
10 commercial products were used. Table 3 summarizes the
gliadin concentrations in 10 commercial products that were
determined using either the developed QCM assay or a
commercial ELISA kit that is approved by AOAC. This
commercial kit is used to detect gliadin using monoclonal
antibodies that recognize the peptide QQPFP. In Table 3, the
first 4 of the 10 food samples were certified gluten-free by the
Spanish Federation of Celiac Association, whereas the others
containing wheat had allergen information concerning wheat at
their packaging. The results of the tests herein reveal that the
AuNP-modified chip can be used to detect gliadin in food
samples because no false-negative result was obtained.
Comparing the gliadin concentrations determined using the
two methods revealed no significant difference for any of the
tested samples. The gluten-free baby rice food product
contained a higher concentration of gluten than the other
three gluten-free products, but the concentration did not

Table 3. Concentration of Gliadin in Food Samples
Determined Using either the Developed QCM Assay or a
Commercial ELISA Kit Approved by AOAC

<table>
<thead>
<tr>
<th>food sample</th>
<th>gliadin concentration (ppm)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>QCM</td>
</tr>
<tr>
<td>gluten-free products</td>
<td></td>
</tr>
<tr>
<td>pancake mix</td>
<td>0.6 ± 0.0</td>
</tr>
<tr>
<td>custard mix</td>
<td>0.9 ± 0.1</td>
</tr>
<tr>
<td>baby rice</td>
<td>8.3 ± 0.8</td>
</tr>
<tr>
<td>buckwheat</td>
<td>0.7 ± 0.1</td>
</tr>
<tr>
<td>wheat-containment products</td>
<td></td>
</tr>
<tr>
<td>rye biscuit</td>
<td>41.0 ± 1.8</td>
</tr>
<tr>
<td>digestive biscuit</td>
<td>55.4 ± 4.8</td>
</tr>
<tr>
<td>plain crackers</td>
<td>53.2 ± 0.4</td>
</tr>
<tr>
<td>red date wheat crispy biscuit</td>
<td>32.2 ± 3.4</td>
</tr>
<tr>
<td>cream cracker</td>
<td>30.8 ± 2.0</td>
</tr>
<tr>
<td>crisp flakes of rice and wheat</td>
<td>44.2 ± 2.8</td>
</tr>
</tbody>
</table>

The gluten-free products had the quality label of “Controlado por
FACE”, which guaranteed that the products are safe for consumption
by persons with celiac disease by the Spanish Federation of Celiac
Associations.

The results in Figure 1 indicate that the 60% ethanol
extraction method in the QCM assay yielded more α-gliadin
than RIDA extraction in the commercial ELISA kit did,
resulting in more gliadin molecules at which the anti-gliadin IgY
could bind. The polyclonal anti-gliadin IgY that was used in the
QCM assay also provided a higher intensity of the signal than
the monoclonal antibody in the commercial ELISA kit did,
because polyclonal antibodies can bind to more than one
epitope per antigen, whereas monoclonal antibodies can bind
to only one epitope per antigen. Accordingly, the different
anti-gliadin antibodies (polyclonal vs monoclonal) in these two
assays might react with different quantities of gliadin, resulting
in slightly different assay results. In Table 4, the sensitivity and

Table 4. Contingency Matrix Obtained from the Change of
Frequency Measured Using QCM for Ethanolic Extracts
from 30 Samples of 10 Foodstuffs (4 “Gluten-Free” and 6
“Gluten-Containing”) Confirmed by an AOAC Approved
ELISA kit

<table>
<thead>
<tr>
<th>actual group</th>
<th>predicted group</th>
<th>gluten-free</th>
<th>gluten-containing</th>
<th>total</th>
<th>sensitivity (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>gluten-free food samples</td>
<td>12</td>
<td>0</td>
<td>12</td>
<td>100</td>
<td></td>
</tr>
<tr>
<td>gluten-containing food samples</td>
<td>0</td>
<td>18</td>
<td>18</td>
<td>100</td>
<td></td>
</tr>
<tr>
<td>total</td>
<td>12</td>
<td>18</td>
<td>30</td>
<td>100</td>
<td></td>
</tr>
<tr>
<td>specificity (%)</td>
<td>100</td>
<td>100</td>
<td>100</td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

specificity of the QCM for 30 samples of the 10 foodstuffs
(4 gluten-free and 6 that contain wheat) were both 100%.
Therefore, the developed QCM biosensor was suited to
identify gliadin contamination in food. It will therefore be
valuable in the manufacture of gluten-free foods and help
ensure compliance with international standards for gluten-free
food.

Conclusion. In this work, a novel, rapid, and sensitive
method for detecting gliadin in gluten-free food using a QCM
biosensor was developed. AuNPs are assembled on a gold electrode in the sensor to detect gliadin. This proposed chip modification increases by 48% the shift in the frequency of the QCM immunosensor in the detection of 2 ppm gliadin. The developed QCM immunosensor had a high sensitivity with a detection limit of 8 ppb gliadin in 60% ethanol. It can be practically utilized for food samples with a detection limit of 1 ppm gliadin. The difference between the LOD of gliadin in 60% ethanol and in food samples may be an effect of the food matrix, because some food compounds, such as lipids or carbohydrates, may interrupt the antibody–antigen interaction, reducing the sensitivity of the assay. The total analysis time was around 40 min, and analyses of gliadin were highly repeatable, with stable results. The developed immunosensor may help food manufacturers to label accurately their gliadin-containing products and may help protect consumers who have allergies to gliadin. Additional research must be performed to improve the AuNP density in the QCM chip.

■ AUTHOR INFORMATION

Corresponding Author
*Postal address: Department of Food Science and Biotechnology, National Chung Hsing University, 250 Kuo Kuang Road, Taichung 402, Taiwan, ROC. Phone: +886-4-22840385, ext. 5020. Fax: +886-4-22876211. E-mail: hwwen@nchu.edu.tw.

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■ REFERENCES
